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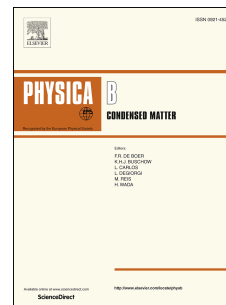
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**Interaction of procarbazine drug and solvent effects on pristine and embedded-zinc oxide  
nanotube as a drug delivery vehicle: A DFT investigation**

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**Abstract**

Numerous research studies have been carried out on nano-structures regarding their potential applications in drug delivery for treating cancers. Within the current work, the procarbazine (PB) drug delivery ability of a pure ZnO nanotube (PZnO-NT) and X-doped (X= Al, Ge, and In) ZnO-NT is inspected through DFT computations. The results demonstrates that PZnO-NT isn't suitable for the PB drug delivery. We showed that doping the Al, Ge, and In atoms into the ZnO-NT structure changes the adsorption energy (AdE) of PB from -6.9 to -26.4, -28.7, and -31.5 kcal/mol, respectively. Moreover, there is a substantial amount of charge transfer from PB to the doped ZnO-NT based on the natural bond orbital analysis. Using water solvent changes the AdE of the drug on the In-doped ZnO-NT from -31.5 to -29.8 kcal/mol. Hence, based on the computations undertaken within this work, the X-doped ZnO-NT can be utilized as a suitable PB carrier.

**Keywords:** ZnO nanotube, Procarbazine drug, Drug delivery, DFT

## 1. Introduction

One of the commonly used anti-cancer medications for the treatment of cancer is procarbazine (PB). Moreover, it is one of the cytotoxic chemotherapeutic drugs used for the treatment of Hodgkin's lymphoma and most brain-related cancers [1]. Being on the WHO list of essential medicines, PB was verified in 1969 for the first time [2-6]. PB is usually taken by mouth. Low blood cell counts, nausea, fatigue, and depression are the common side effects associated with PB [7, 8]. It is possible to use drug delivery systems (DDSs) in order to overcome such drawbacks [9]. DDSs have enjoyed considerable attention owing to their significant in drug delivery to target cells [10]. However, low drug loading efficiency, high toxicity, and immunogenicity are some of the major drawbacks to many of these systems [11, 12]. Researchers have investigated nanocarriers in order to correct the defects in anti-cancer drugs such as lack of selectivity, severe toxicity, low water solubility, and severe side effects [13-16].

Nowadays, nanotechnology is helping to significantly advance and revolutionize numerous technology and industry sectors, including information technology, food safety, environmental science [17-22], transportation, medicine, and energy [23-26]. Many research groups and scientists have found that one-dimensional (1D) nanostructures are encouraging DDSs for many drugs [27]. The most widely employed 1D nanostructures as DDSs are carbon nanotubes (CNTs) [28]. Nonetheless, many chemicals have a weak interaction with pure CNTs. This makes it almost impossible to employ CNTs as ideal DDSs [29, 30]. So, methods such as doping of impurities, chemical functionalization and generation of structural defects were adopted to resolve the above-mentioned problem [31-34]. Furthermore, impurity atoms such as Zn or O have been substituted for C atoms in diverse C-like nanotubes [35, 36]. One of the most commonly used nano-structures is ZnO nanotube (ZnO-NT), which has been successfully synthesized [37]. The ZnO-NT has a

large bandgap and polar Zn-O bonds, demonstrating its potential application in semiconductor-based DDSs. There are numerous studies on the interaction between ZnO-NT and different chemical agents. A pure ZnO-NT (PZnO-NT) cannot be considered as a suitable DDS in most cases because its stability is high and its tendency to have a reaction with different chemicals is less. Nonetheless, manipulating the structure of nanomaterials have been shown to be effective in boosting their reactivity to different chemicals [38, 39]. Here, density functional theory (DFT) computations are undertaken to investigate the interaction between PB and PZnO-NT, and X-doped (X = Al, Ge, and In) ZnO-NTs (X@ZnO-NTs) to find a DDS.

## 2. Computational details

In order to precisely describe the molecular properties of nanostructures, one of the commonly used density functionals is B3LYP. Nevertheless, estimation of dispersion interactions is one of its main drawbacks. Hence, we assessed the dispersion forces by including the Grimme's "D" [40]. The basis set (BS) utilized in this study is 6-31++G\*\* (d) and the software used to undertake the computations is GAMESS [41]. The LANL2DZ BS is applied for the transition metals [42]. Moreover, the GaussSum program is used for the drawing of density-of-states (DOS) diagrams [43]. Based on the previous studies, B3LYP is one of the common functionals used to describe nanostructures due to its high accuracy [44, 45]. We computed the adsorption or adhesion energy (AdE) related to a PB drug on the nanotube surface through Eq. 1:

$$\text{AdE} = E(\text{PB}/\text{ZnO-NT}) - E(\text{PB}) - E(\text{ZnO-NT}) + E_{\text{BSSE}} \quad (1)$$

where  $E(\text{PB}/\text{ZnO-NT})$  represents the energy of the ZnO-NT onto which a PB molecule was adhered.  $E(\text{PB})$  is the energy of PB.  $E(\text{ZnO-NT})$  is the energy of the pure ZnO-NT.  $E_{\text{BSSE}}$  has been computed by adopting the counterpoise method for all interactions [46]. The harmonics have been

estimated to verify that all geometries have positive frequencies. Eq. 2 was used to estimate the bandgap between the HOMO and the LUMO:

$$E_g = E_{\text{LUMO}} - E_{\text{HOMO}} \quad (2)$$

where  $E_{\text{LUMO}}$  and  $E_{\text{HOMO}}$ , respectively, are the energies of the lowest unoccupied and the highest occupied molecular orbitals.

### 3. Results and discussions

#### 3.1. The characteristics of the nanotube and PB

The PB adhesion onto the nanotube surface (Fig. 1) was examined by choosing a ZnO-NT model (36 Zn and 36 O atoms). ZnO-NTs have been previously employed to adsorb various chemicals such as NO, N<sub>2</sub>O<sub>2</sub>, CO<sub>2</sub>, CO, H<sub>2</sub>O<sub>2</sub>, N<sub>2</sub>O, and NH<sub>3</sub> [47-50]. Moreover, the predicted diameter of ZnO-NT and the Zn-O bond length have been 8.81, and 1.92 Å, respectively, which were similar to those in experimental studies, i.e., 1.92 Å for Zn-O bond length [47]. According to the DOS diagram in Fig. 1, the LUMO energy is -2.54 and the energy of the HOMO is -6.36 eV for ZnO-NT (Table 1). So, the energy gap is around 3.82 eV. According to Fig. 2, there are several functional groups on the hexagonal ring of PB. We observed an HOMO profile within the PB structure, a site which was suitable for attacking the Zn atoms of ZnO-NT (Fig. 2).

#### 3.2. The interaction between PZnO-NT and PB

The initial stage in DDSs is the adhesion of a drug to a carrier. We explored the PB adhesion on the PZnO-NT. The adhesion of PB on PZnO-NT is examined by placing a PB molecule at different sites (i.e., over Zn or O atoms, over a hexagon center and over the bridge of bonds). The PB was positioned on the PZnO-NT perpendicularly or in a parallel manner. According to Fig. 3, after the

initial geometry optimization, three local minima are predicted. The adhesion energy values of all complexes (CMPLs, Table 1) revealed that the PB adhesion to the ZnO-NT is weak and AdE ranges from -5.2 to -6.9 kcal/mol.

According to Fig. 3, in CMPL **T** (the CMPL with most stability), PB has a perpendicular interaction with the ZnO-NT surface and the distance is 3.76 Å for one O atom, and adhesion energy is -6.9 kcal/mol. As shown, PB somehow shared the O lone pairs with the Zn atoms. The NBO charge transfer from PB to the nanotube was 0.09 |e|, indicating the physical adhesion of PB to the ZnO-NT. There was a decrease in the bandgap from 2.82 eV in the PZnO-NT to 3.50 eV in CMPL **T**. The data for other CMPLs are provided in Table 1 and Fig. 3. The more stability of the CMPL **T** than another CMPLs can be ascribed to the HOMO of PB which was chiefly located on the O atom. As provided in Table 1, not any appreciable change occurred in the electronic attributes of ZnO-NT following the adhesion of PB. In addition to this, the less negative adhesion energy values, the very low adhesion capacity of ZnO-NT and the weakness of the interaction. Hence, the possibility of using the pure ZnO-NT as a proper nanocarrier for PB is low. The ZnO-NT was doped with the X atom to resolve the problem and boost the adhesion capacity and the interaction strength.

#### *3.4. X-doping in the ZnO-NT structure*

In order to boost the low reactivity of ZnO-NT towards PB, an X atom was substituted for O (NT **E**) and Zn atoms (NT **F**) in the ZnO-NT. Then, its impact was inspected on the electronic attributes and the geometric structure (GS) of the ZnO-NT (Fig. 4). The X atom caused a disruption in the ZnO-NT structure because the size of X atom is larger than the size of Zn and O atoms. This caused the X atom to project out of the surface of the ZnO-NT.

We inspect the stability of X-doped ZnO-NT (X@ZnO-NT) by computing the standard enthalpy of formation ( $\Delta_f H^0$ ). Subtracting the deliberate atomization energy ( $\Sigma D_0$ ) from the separated atoms' known enthalpy of formation yielded the theoretical enthalpy of formation at 298 K. For any X@ZnO-NT,  $\Delta_f H^0$  at 298 K for one atom was given by [51]:

$$\Delta_f H^0 (\text{X@ZnO-NT}) = \Delta_f H^0 (\text{X}) + r \Delta_f H^0 (\text{Zn}) + t \Delta_f H^0 (\text{O}) - \Sigma D_0 \quad (3)$$

Here,  $r$  is the number of Zn atoms and  $t$  is the number of O. The estimated  $\Delta_f H^0$  for Al, Ge, and In replaced instead of O atom in ZnO-NT, respectively, was -79.5, -82.4, and -97.1 kcal/mol.  $\Delta_f H^0$  for Al, Ge, and In replaced instead of Zn atom in ZnO-NT, respectively, was -84.2, -91.3, -100.3 kcal/mol. In conclusion, NT **F** was thermodynamically more stable than NT **E**. Equation 4 was used to compute the standard Gibbs free energy of formation ( $\Delta_f G^0$ ) for these two NTs in order to understand the entropic effect on their stability:

$$\Delta_f G^0 (\text{In@ZnO-NT}, 298 \text{ K}) = \Delta_f H^0 (\text{In@ZnO-NT}, 298 \text{ K}) - 298 \Delta S \quad (4)$$

Here,  $\Delta S$  is the change in entropy. The estimated  $\Delta_f G^0$  for NTs **E** and **F** (In@ZnO-NT), respectively, was -18.9 and -50.3 kcal/mol, respectively. Here, the negative values demonstrate that the formation of In@ZnO-NT from the atoms is favorable thermodynamically, particularly in the NT **F**, in which a Zn atom was replaced by an X atom. The electron transfer from O atoms to the metal atoms could be the possible reason for the greater stability of NT **F** than NT **E**. Thus, NT **F** was selected to see how PB was adsorbed. The length of Al-O, Ge-O, and In-O bonds are about 2.95, 3.08, and 3.34 Å, respectively, in NT **F**. These bonds were longer compared to Zn-O bonds. Doping the X atom appreciably reduced the bandgap of ZnO-NT (see Table 2) thanks to the appreciable change in the HOMO to lower energies following X-doping. After its doping, the X@ZnO-NT changed into a p-type semiconductor.



Different orientations were taken into account to place a PB above the X atom to inspect the interaction between PB and the X@ZnO-NT (NT F). Following the optimization of structures, one of the orientations was a local minimum, namely; PB/X@ZnO-NT (Fig.5). In this CML, the PB was placed at the top of the X atom with the bond length of 3.11, 3.03, and 2.92 Å for PB/Al, Ge, In@ZnO-NT, respectively. According to the NBO analysis, the partial positive charge of Al, Ge, and In was 0.64, 0.67, and 0.73 |e|, respectively. As a result, the PB could be adhered onto the X atom from the O atom PB (HOMO head) (Fig. 2). For PB/Al, Ge, In@ZnO-NT, the AdE is -26.4, -28.7, and -31.5 kcal/mol, respectively. Based on the results, doping the X atom led to an appreciable increase in the reactivity of the ZnO-NT toward the PB in comparison with the PZnO-NT. Electronic property analysis was carried out to verify this.

According to Table 2, a change was observed in the electronic attributes of the X@ZnO-NT following the adhesion of PB. The NBO charge transfer of about 0.26, 0.31, and 0.37 |e| occurred from the drug to the Al, Ge, and In, respectively. There was substantial destabilization in the HOMO level of X@ZnO-NT in the range of 27 to 34% following the adhesion of PB (see Table 2, and Fig. 6 for In@ZnO-NT). This substantial destabilization could be due to the nucleophilic nature of PB attacking the HOMO of the X@ZnO-NT (Fig. 7), which led to a substantial change in its energy. Nonetheless, modifying the electronic attributes of a material is one of the effective ways for DDSs and electronically harmless adhesion processed are considered ideal.

### 3.5. The influence of solvent on the adhesion

The solute-solvent interactions are responsible for the significant changes in the chemical and physical characteristics of the solute in going from gas phase to solvent phase [52-54]. Here, the influence of the H<sub>2</sub>O solvent (HS) on the adhesion of PB to the In@ZnO-NT (for instance) was

inspected through the PCM [55]. For this purpose, the structures of PB, In@ZnO-NT, and CMP of PB/In@ZnO-NT were reoptimized in the HS. The findings revealed that the adhesion got weak and a change was observed in adhesion energy from -31.5 to -29.8 kcal/mol. Thus, it could be expressed as Eq. 3:

$$\Delta E_{\text{solv-gas}} = \text{AdE (HS)} - \text{AdE (gaseous phase)} = 1.7 \text{ kcal/mol} \quad (3)$$

here  $\Delta E_{\text{solv-gas}}$  denotes the differences between the adhesion energy of PB in the gaseous phase (G-P) and in the HS.  $\Delta E_{\text{solv}}$  (energy of solvation) of PB, In@ZnO-NT, and PB/In@ZnO-NT CMPs was calculated using Eq. 4:

$$\Delta E_{\text{solv}} = E_{\text{solv}} - E_{\text{gas}} \quad (4)$$

Here, the energies of a species in the G-P and in the HS and are represented by  $E_{\text{gas}}$  and  $E_{\text{solv}}$ , respectively. The  $\Delta E_{\text{solv}}$  of In@ZnO-NT, PB, and PB/In@ZnO-NT, respectively, are -11.1, -6.1, and -12.2 kcal/mol, which demonstrate that the sum of  $E_{\text{solv}}$  of In@ZnO-NT and PB was more negative than the  $E_{\text{solv}}$  of PB/In@ZnO-NT. Indeed, In@ZnO-NT and PB were highly polar with an electric dipole moment, which made them more soluble in the polar HS. Hence,  $\text{H}_2\text{O}$  molecules surrounded PB and In@ZnO-NT forcefully, thus, preventing their interactions. Unlike in the GP, there was a slight change in the bandgap of In@ZnO-NT following its interaction with PB in the HS (around -0.09 eV). So, a negligible decrease was observed in the sensing response of In@ZnO-NT to PB in the HS.

### 3.6. The release of PB

The X@ZnO-NT is ideal for the adhesion of PB, which is the most pivotal step in DDSs. However, one of the challenges in DDSs is the release of drug from a carrier in target cells. The pH of normal cells is in fact more than the pH of tumor cells, showing that the environment of tissues has a pH

below 6 [56]. The influence of pH on the CMP (with most stability) between the In@ZnO-NT (for example) and PB was examined. We assume that  $H^+$  species tend to attach to the nucleophilic heads of PB. So, we protonated the O atom of PB and performed the optimization computations. As a result, the AdE changes in the acid milieu from -31.5 to -20.2 kcal/mol and the distance between PB and the In@ZnO-NT increases to 3.54 Å. Also, according to Fig. 8, the interaction nature changes from a covalent bond (CB) to the H-bond (HB), which separates PB from the carrier via protonation. The protonated PB could not attach to the carrier, and it had to be released.

#### 4. Conclusions

The potential use of PZnO-NT and X@ZnO-NT as drug carriers was investigated by examining the adhesion of PB to their surface. The interaction of PZnO-NT with PB was weak. However, after doping the X atom, the O atom of PB interacted with the X atom of the Al, In and Ge with AdE of about -26.4, and -31.5 and -28.7 kcal/mol, respectively. The mechanism of interaction changed from CB in blood cells to HB in cancerous cells, which could separate PB from In@ZnO-NT in cancerous cells with a low pH via protonation. The HB energy was very low, which was about -20.2 kcal/mol. The PCM was used to examine the solvent effect on the drug AdE on the In@ZnO-NT, indicating that it is about -29.8 kcal/mol. Overall, the results suggested the potential use of X@ZnO-NT (especially In@ZnO-NT) as an encouraging nanocarrier for PB delivery.

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**Figure captions**

**Figure 1.** Optimized structure of the ZnO nanotube (ZnO-NT) and its density of states (DOS).

Distance is in Å.

**Figure 2.** Optimized structure of procarbazine (PB) drug and its HOMO profile.

**Figure 3.** Optimized structures of PB/ZnO-NT complexes. Distances are in Å.

**Figure 4.** Optimized structures of different X atom-doped ZnO-NT (X@ZnO-NT).

**Figure 5.** Optimized structures of PB/Al, Ge, and In@ZnO-NT complexes. Distances are in Å.

**Figure 6.** Partial DOS of the most stable PB/In@ZnO-NT complex.

**Figure 7.** The HOMO profile of the most stable PB/In@ZnO-NT complex.

**Figure 8.** The optimized structure of protonated PB and In@ZnO-NT, showing separation from each other in the acidic environment. Distance is in Å.

**Table 1.** The calculated adsorption energy (AdE) in kcal/mol, HOMO, LUMO energies, and HOMO-LUMO energy gap ( $E_g$ ) of bare ZnO nanotube (ZnO-NT) and the procarbazine (PB) and ZnO-NT complexes in eV. Q is the charge on the molecules.

Structure	AdE	$E_{\text{HOMO}}$	$E_{\text{LUMO}}$	$E_g$	$\Delta E_g(\%)$	Q(e)
ZnO-NT	-	-6.36	-2.54	3.82	-	-
<b>R</b>	-5.2	-6.14	-2.54	3.60	-5.8	0.06
<b>S</b>	-6.1	-6.09	-2.53	3.56	-6.8	0.07
<b>T</b>	-6.9	-6.02	-2.52	3.50	-8.4	0.09

**Table 2.** The calculated adsorption energy (AdE) kcal/mol, HOMO, LUMO energies, and HOMO-LUMO energy gap ( $E_g$ ) of X-doped ZnO-NT (X = Al, Ge, and In and X@ZnO-NT) and the PB complexes in eV. Q is the charge on the molecules.

Structure	AdE	$E_{\text{HOMO}}$	$E_{\text{LUMO}}$	$E_g$	$\Delta E_g(\%)$	Q(e)
Al@ZnO-NT	-	-5.15	-2.51	2.64	-	-
PB/Al@ZnO-NT	-26.4	-4.41	-2.49	1.92	-27.3	0.26
Ge@ZnO-NT	-	-5.12	-2.52	2.60	-	-
PB/Ge@ZnO-NT	-28.7	-4.28	-2.49	1.79	-31.2	0.31
In@ZnO-NT	-	-5.08	-2.48	2.60	-	-
PB/In@ZnO-NT	-31.5	-4.16	-2.45	1.71	-34.2	0.37

Figure 1.

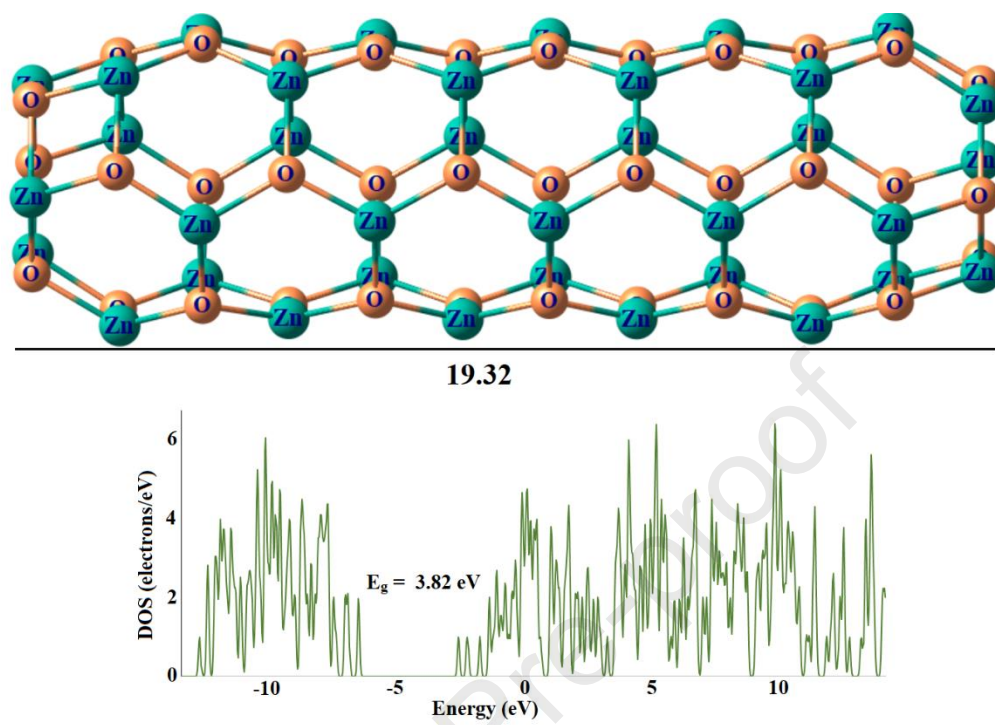


Figure 2.

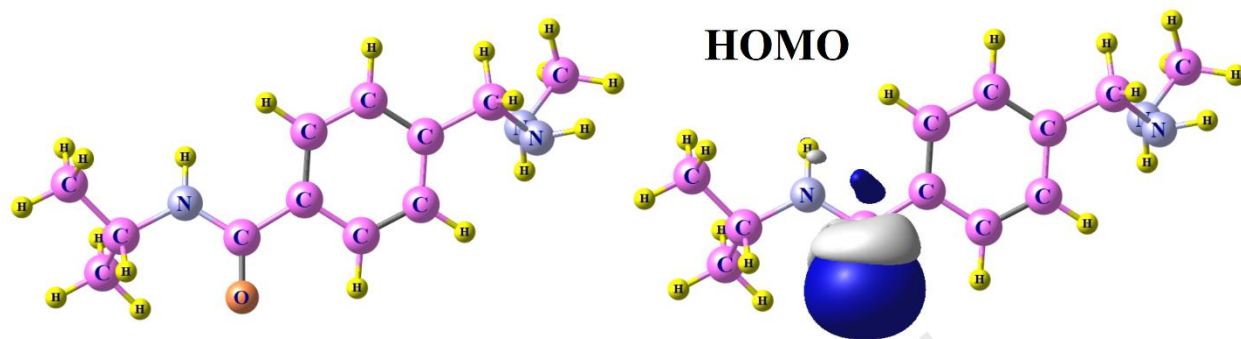




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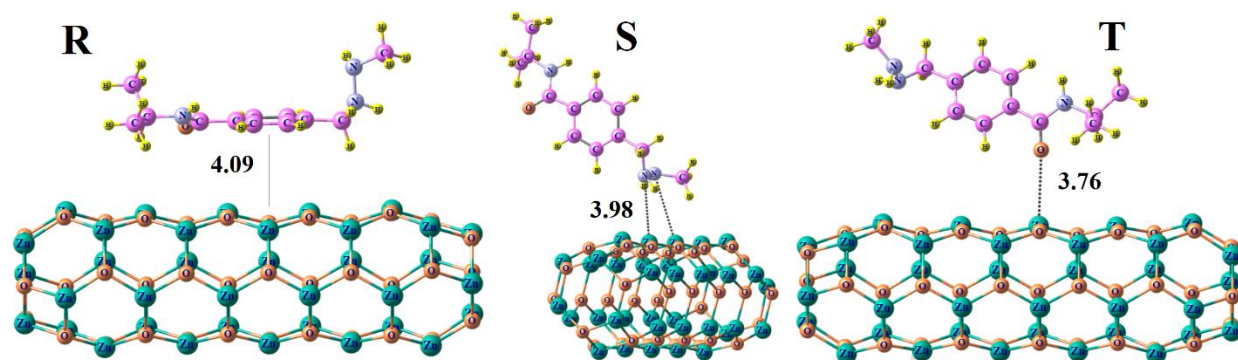


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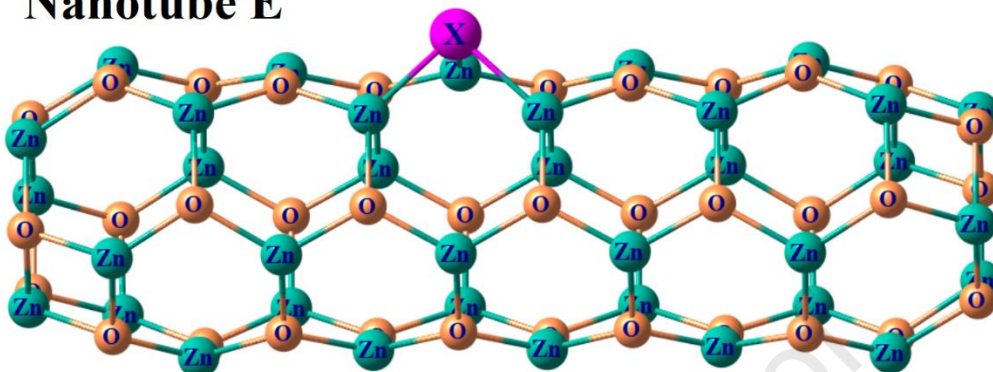
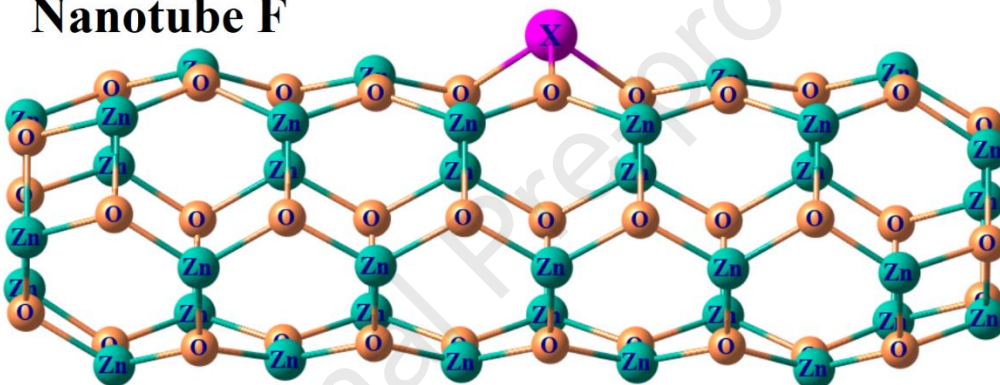
**Nanotube E****Nanotube F**

Figure 5.

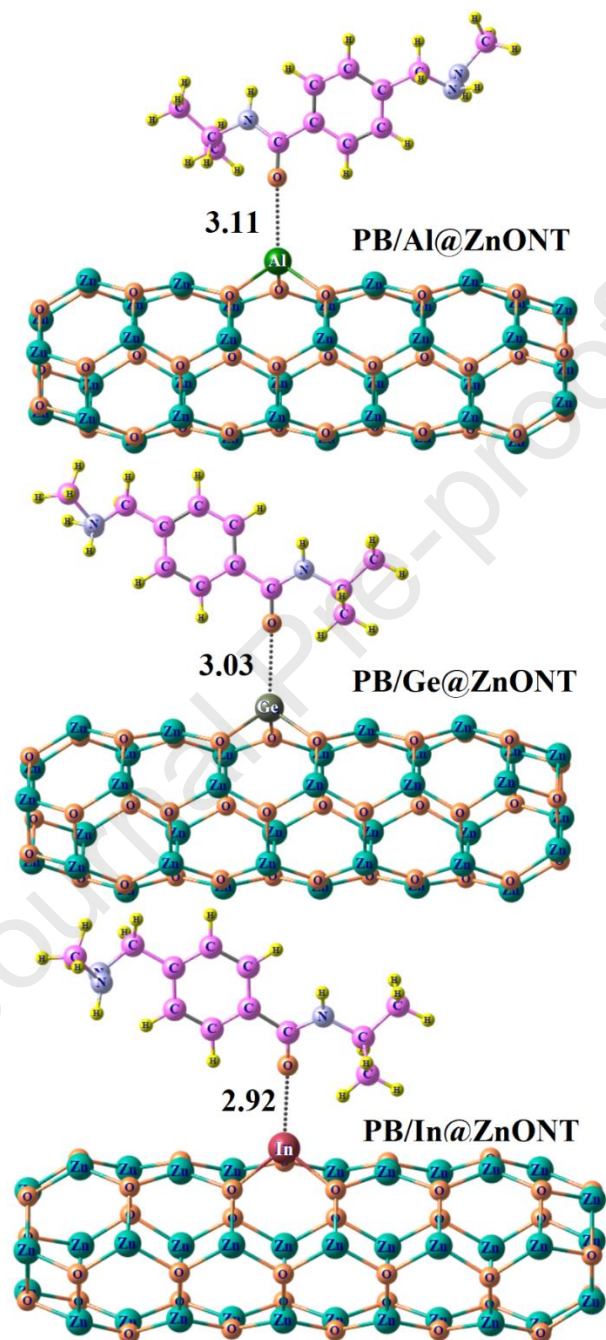


Figure 6.

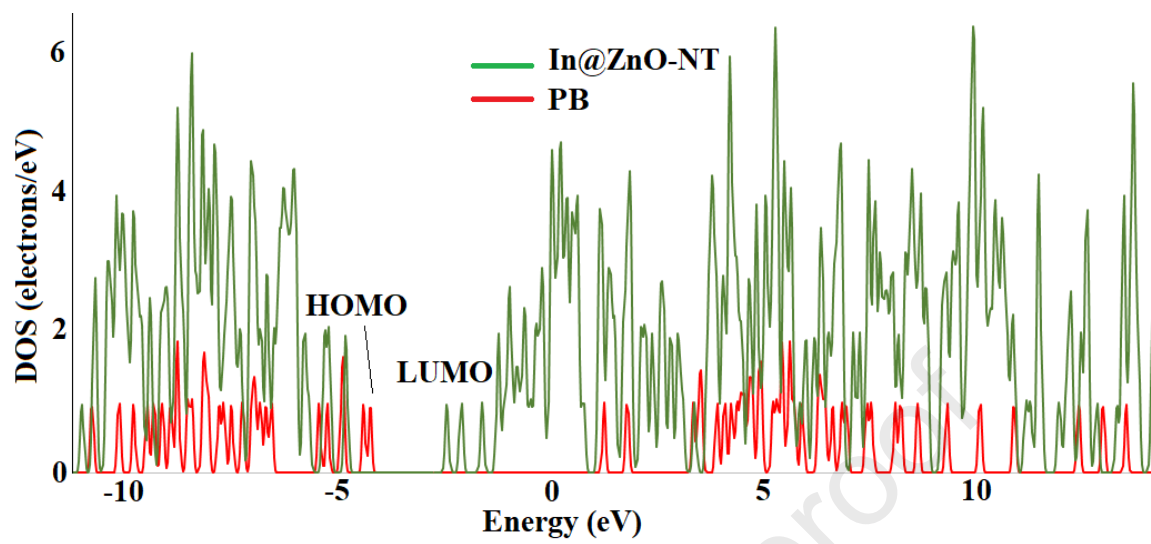


Figure 7.

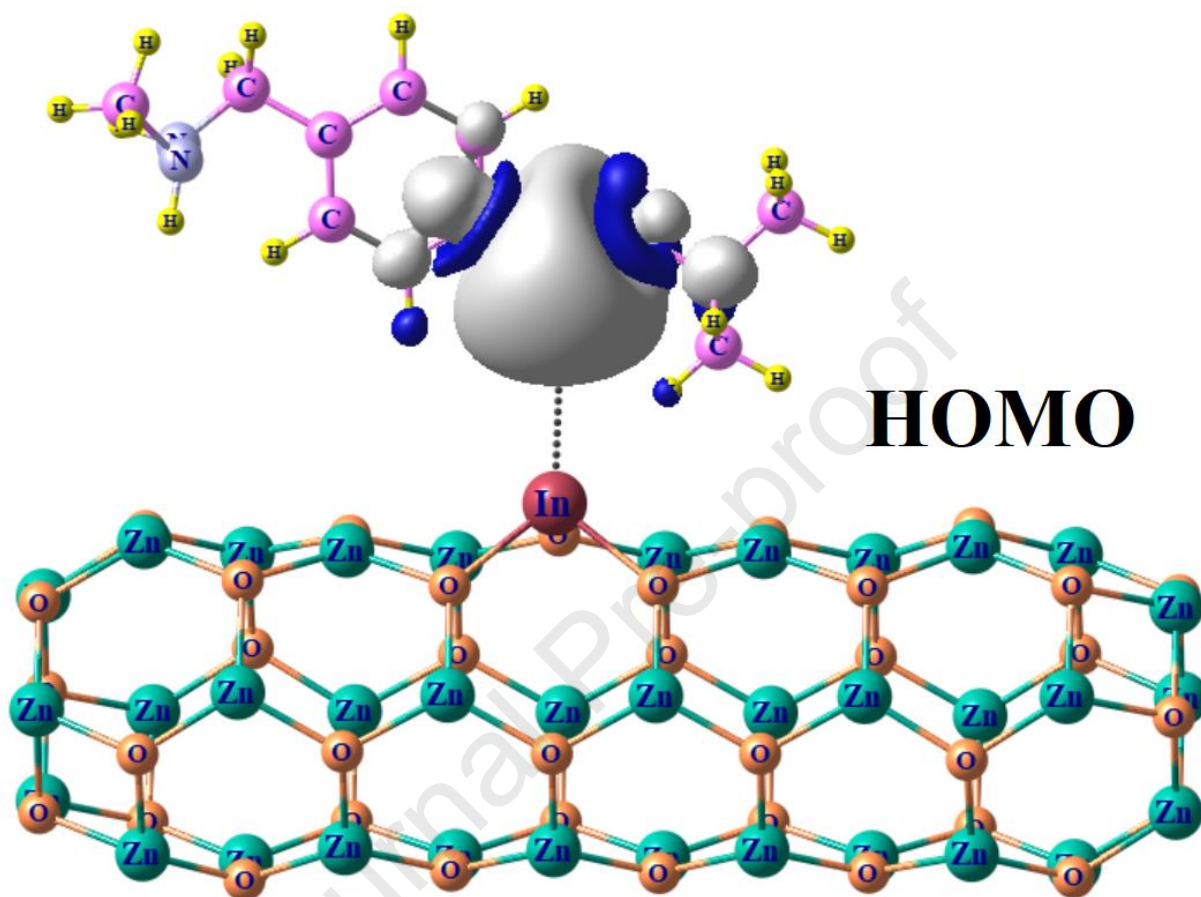
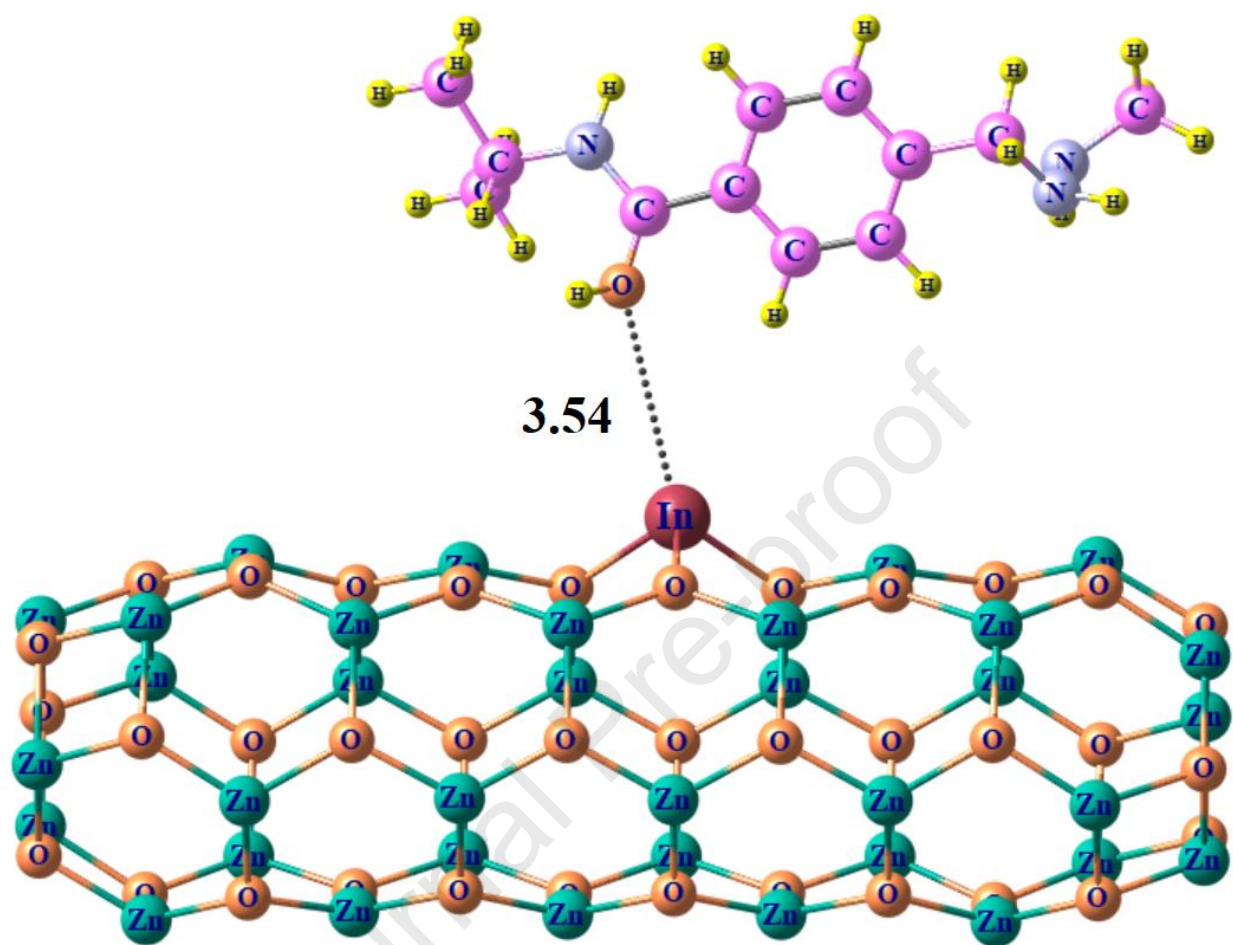


Figure 8.



**Declaration of interests**

The authors declare that they have no known competing financial interests or personal relationships that could have appeared to influence the work reported in this paper.

The authors declare the following financial interests/personal relationships which may be considered as potential competing interests:

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